

# MODELLING THE THREE-POINT BENDING OF NOVEL BIOINSPIRED DENTAL CROWN COMPOSITES

U. Jargalsaikhan<sup>1</sup>, H. Wan<sup>2</sup>, N. Leung<sup>1</sup>, B. Su<sup>2</sup>, X. Song<sup>3</sup>, J. Hu<sup>4</sup>, T. Sui<sup>1\*</sup>  
<sup>1</sup> Bioinspired Materials Group, Department of Mechanical Engineering Sciences, University of Surrey, Guildford, Surrey, UK,  
<sup>2</sup> Biomaterials Engineering Group (bioMEG), Bristol Dental School, University of Bristol, Bristol, U.K.,  
<sup>3</sup> Department of Mechanical and Automation Engineering, Chinese University of Hong Kong, Shatin, Hong Kong, China,  
<sup>4</sup> Sente Software Ltd., 40 Occam Road, Surrey Technology Centre, Guildford, Surrey, UK  
 \* Corresponding author: [t.sui@surrey.ac.uk](mailto:t.sui@surrey.ac.uk)

## 1. Background

### Dental CARIES: a Global Issue



Figure 1.1. Dental hard tissue loss, a. Sound enamel, b. Initial lesion, c and d. Extensive lesion [1].

Caries is the major cause of dental hard tissue damage and teeth loss. It is an **infectious, chronic** disease that has affected **millions** of people globally [2].

- **3.2 billion** people worldwide are affected by oral disease (2019) [2].
- **22 million** adults were seen by an NHS dentist in England (2018) [3].
- **9.7 million** treatment courses in one quarter of 2018-2019 [3].
- **20%** of ceramics used as top layers fail within the first 5 years of use [4].

### Current Treatment Solutions

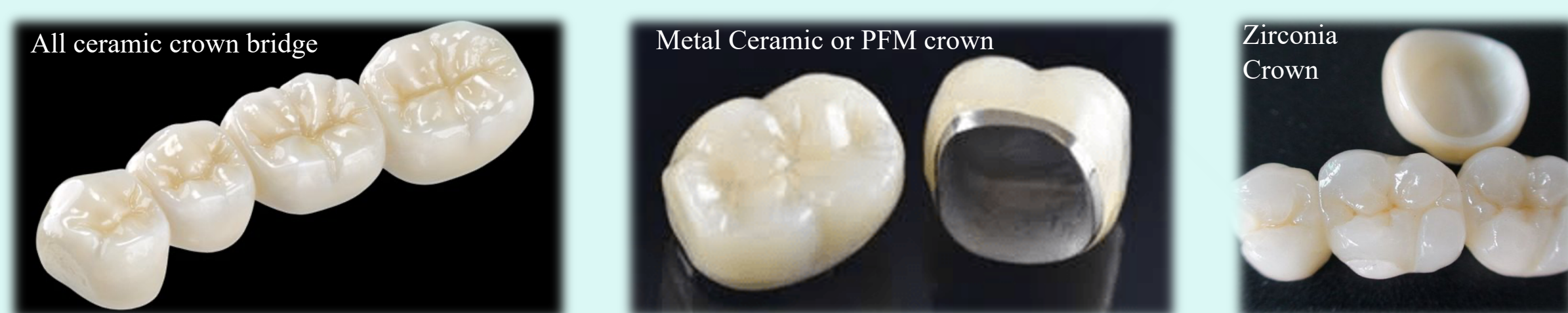


Figure 1.2. Commercial dental crown materials

### Novel Dental Crown Materials Inspired by Nature

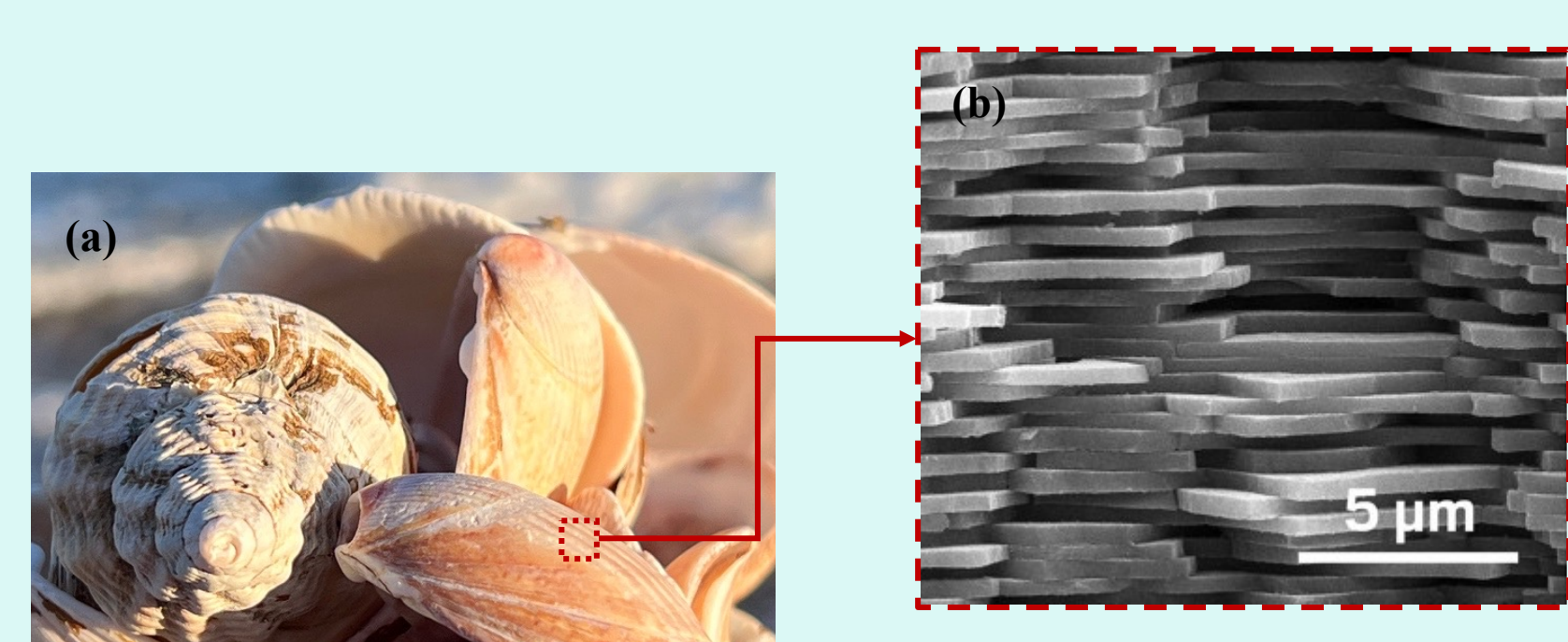


Figure 1.3 (a) Natural nacre. (b) Nacre layered structure acquired by SEM [5].

- Nature designs a perfect complex structure in living organisms on a **macro and nano-level**.
- The hierarchical structure of natural teeth is overly complex for our current manufacturing techniques.
- However, nacre (known as mother of pearl) has a simpler microstructure of **aragonite** platelets held together by **proteins** that provide good strength and fracture resistance [6].

## 2. Materials and Methodology

Bioinspired alumina ( $\text{Al}_2\text{O}_3$ ) scaffolds were achieved by using a **cost-effective**, bi-directional freeze-casting technique. It was later densified, sintered and polymer infiltrated as described in [7]. The four different polymers used in this study are:

- Polymethyl methacrylate (PMMA)
- Urethane dimethacrylate/Triethylene glycol dimethacrylate (UDMA/TEGDMA)
- Polyurethane (PU)
- Epoxy.

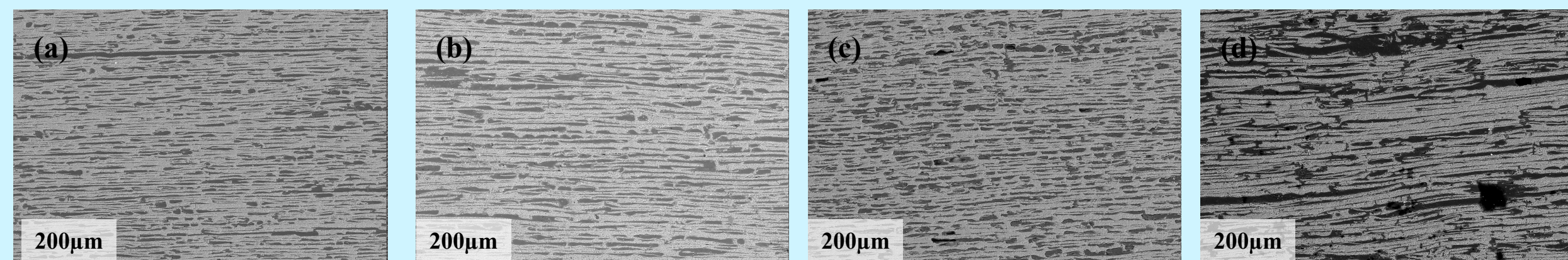


Figure 2.1 The microstructure SEM images of  $\text{Al}_2\text{O}_3$  composites with different polymer phases. (a)  $\text{Al}_2\text{O}_3$ /PMMA, (b)  $\text{Al}_2\text{O}_3$ /UDMA-TEGDMA, (c)  $\text{Al}_2\text{O}_3$ /PU and (d)  $\text{Al}_2\text{O}_3$ /epoxy.

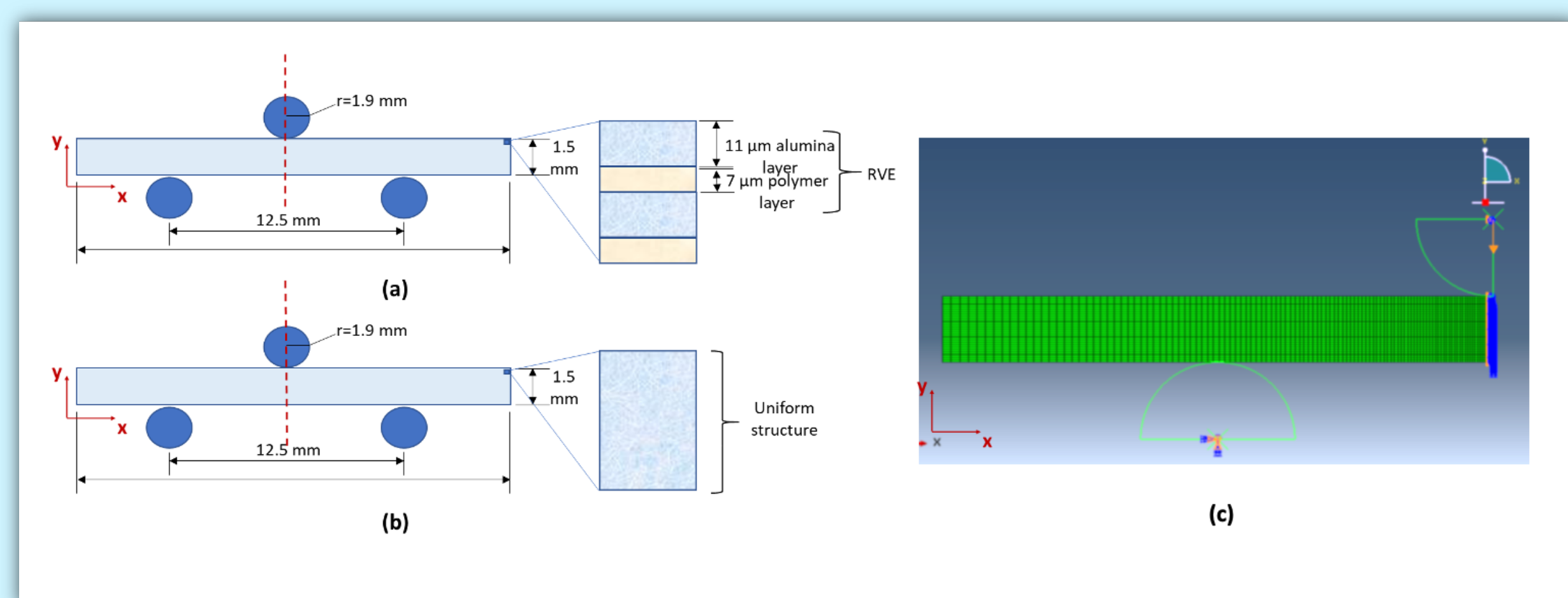


Figure 2.2 A schematic diagram of the three-point bending test. (a) The geometry equivalent uniform structure model, (b) Bioinspired multi-layer structure, (c) 2D axisymmetric three-point bending boundary conditions used in FEM.

The FEM simulations were carried out using the commercial finite element software, ABAQUS® (version 6.4.2, 2018). Two types of models were proposed using the same finite element framework:

- Bioinspired multi-layer model
- Equivalent uniform structure model, without a layered architecture, to compare the stress distributions in the four composites.

Constant displacement of 0.7 mm applied on the top pin and 2D 4-node bilinear plane strain quadrilateral elements (CPE4R) were used to simulate the model.

## 4. Conclusion and Future Work

The present study focused on stress distributions in bioinspired multi-layer  $\text{Al}_2\text{O}_3$  composites and compared them with an equivalent uniform structure model using 2D FEM modelling. The  $\sigma_{avg}$  in multi-layer models is lower than that of the equivalent uniform structure models.

In addition, polymer associated differences were identified in  $\sigma_{avg}$ . This modelling technique requires less computational memory along with faster convergence, meaning it can be beneficial in optimising polymer composition for further 3D modelling to investigate tri-axial stress state. Thus, it will develop better understanding on the mechanical performance of a novel, bioinspired,  $\text{Al}_2\text{O}_3$  based dental crown material.

## Acknowledgements

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## 3. Results and Discussion

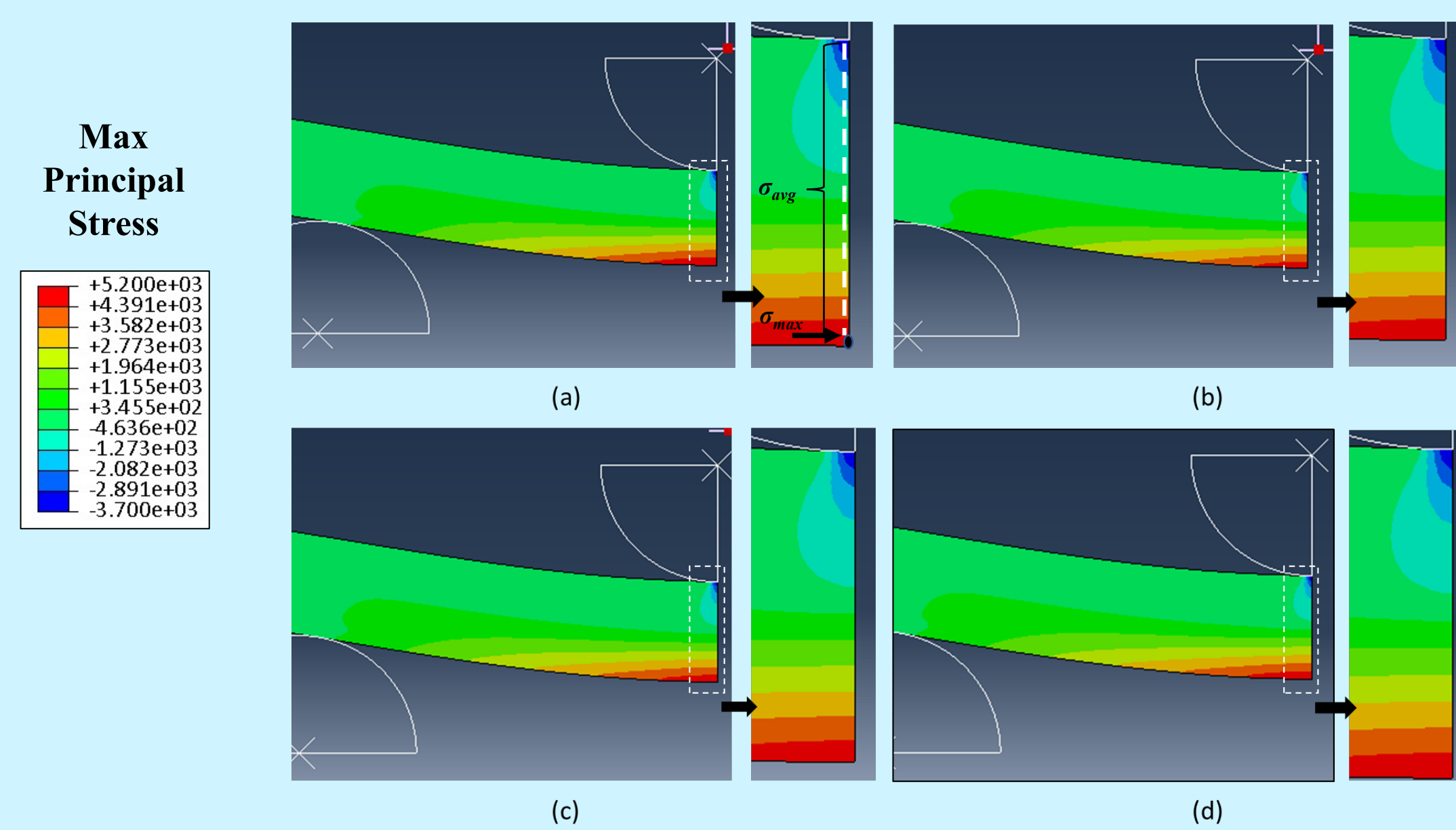


Figure 3.1 Principal stress distribution in equivalent uniform structure models of  $\text{Al}_2\text{O}_3$  composites. The central region of the model magnified to show the stress concentration area. (a)  $\text{Al}_2\text{O}_3$ /PMMA, (b)  $\text{Al}_2\text{O}_3$ /UDMA-TEGDMA, (c) PU, (d)  $\text{Al}_2\text{O}_3$ /epoxy. The scale bar is in MPa. With insert image of high magnification of stress concentrated area.

The average stress ( $\sigma_{avg}$ ) value was calculated from the central line nodes under the top pin. According to the statistical analysis, there was a statistically significant difference in  $\sigma_{avg}$  between equivalent uniform structure models and bioinspired multi-layer models ( $p \leq 0.05$ ).

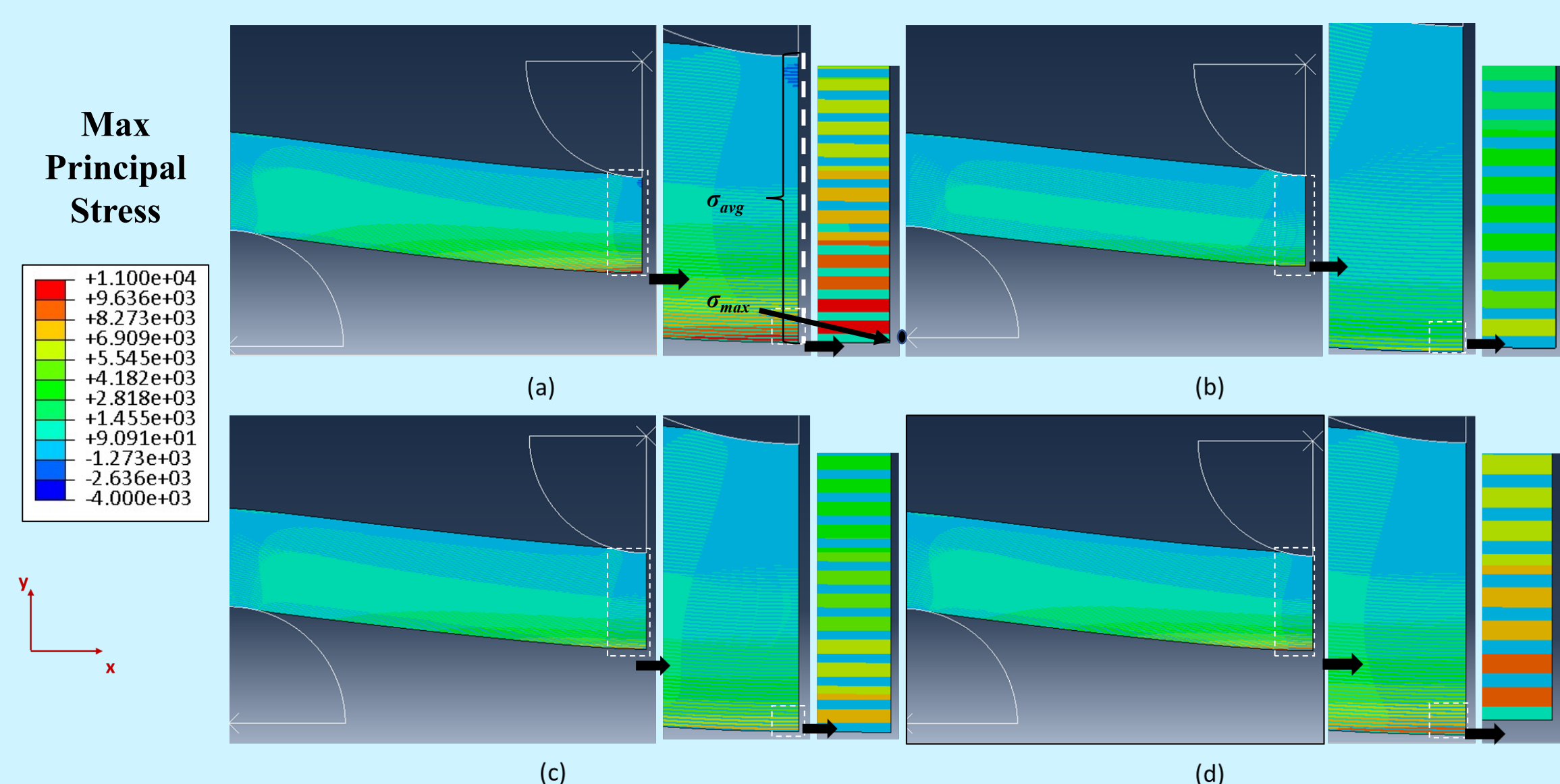


Figure 3.2 Principal stress distribution in bioinspired multi-layer structure models of alumina-based composites. The central region of the model magnified to show the stress concentration area. (a)  $\text{Al}_2\text{O}_3$ /PMMA, (b)  $\text{Al}_2\text{O}_3$ /UDMA-TEGDMA, (c) PU, (d)  $\text{Al}_2\text{O}_3$ /epoxy. The scale bar is in MPa.

In each model, the differences between polymer components'  $\sigma_{avg}$  is minimal in equivalent uniform structure models, whereas it is significantly higher in bioinspired multi-layer models ( $p \leq 0.05$ ). The  $\text{Al}_2\text{O}_3$ /PMMA composites displayed higher  $\sigma_{avg}$  than  $\text{Al}_2\text{O}_3$ /UDMA-TEGDMA and  $\text{Al}_2\text{O}_3$ /PU composites ( $p \leq 0.05$ ). However, a statistically significant difference was not found between the  $\sigma_{avg}$  of the  $\text{Al}_2\text{O}_3$ /PMMA and  $\text{Al}_2\text{O}_3$ /epoxy composites ( $p \leq 0.05$ ).

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